# Convergence & Non-Convergence of Algebraic Iterative Reconstruction Methods

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Joint work with

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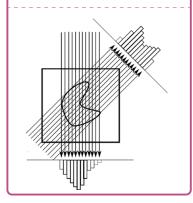


- X-ray CT model
- Stationary iterative reconstruction methods
- Their convergence
- Semi-convergence with noisy data
- Unmatched projectors
- Non-convergence and how to avoid it
- Fixing stationary methods
- Krylov subspace methods  $\rightarrow$  GMRES

# Prelude: X-Ray CT and the Radon Transform

#### The Principle

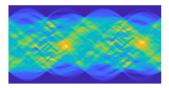
Send X-rays through the object f at many angles, and measure the attenuation g.



f = 2D object/image



 $g = \mathcal{R} f =$ Radon transform of f= sinogram



$$\mathcal{B} = \operatorname{adjoint}(\mathcal{R})$$

# Reconstruction Algorithms

### **Transform-based methods**

- Formulate the forward problem as a certain *transform*, then formulate a stable way to *invert* the transform.
- 2D parallel-beam CT: Radon transform  $\leftrightarrow$  filtered back projection.
- Tailored to specific measurement geometries.
- Works well with lots of data.

### Algebraic methods

- Discretize the forward problem and solve the corresponding large-scale problem Ax = b by means of an *iterative method*.
- Works for any measurement geometry.
- Can work well with limited data.

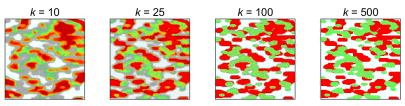
The simplest method: Landweber = steepest descent

$$x^{k+1} = x^k + \omega A^T (b - A x^k), \qquad k = 0, 1, 2, \dots$$

# Example of Convergence for Landweber

Image size:  $128 \times 128$ . Data: 360 projection angles in  $[1^{\circ}, 360^{\circ}]$ , 181 detector pixels.





We must be concerned with three types of convergence:

- Convergence of the iterative method.
- Semi-convergence in the face of noisy data.
- **Non-convergence** when forward and back projections don't match.

# Asymptotic Convergence for Landweber

#### Follows from Nesterov (2004)

Assume that A is invertible and scaled such that  $||A||_2^2 = m$ .

$$\|x^{k} - \bar{x}\|_{2}^{2} \leq \left(1 - \frac{2}{1 + \kappa^{2}}\right)^{k} \|x^{0} - \bar{x}\|_{2}^{2},$$

where  $\bar{x} = A^{-1}b$  and  $\kappa = ||A||_2 ||A^{-1}||_2$ . This is linear convergence.

When  $\kappa$  is large then we have the approximate upper bound

$$\|x^k - \bar{x}\|_2^2 \lesssim (1 - 2/\kappa^2)^k \|x^0 - \bar{x}\|_2^2$$
,

showing that in each iteration the error is reduced by a factor  $1 - 2/\kappa^2$ .

### Real Problems Have Noisy Data

A standard topic in numerical linear algebra: solve Ax = b. Don't do this for inverse problems with noisy data!

The right-hand side b (the data) is a sum of noise-free data  $\overline{b} = A \overline{x}$  from the ground-truth image  $\overline{x}$  plus a noise component e:

$$b = A \bar{x} + e, \quad \bar{x} =$$
ground truth,  $e =$  noise.

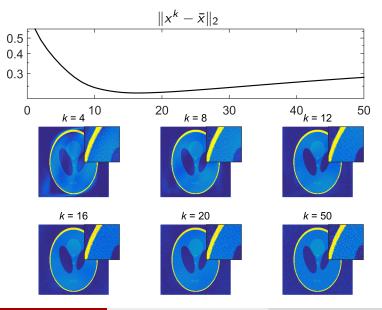
The naïve solution  $x^{\text{naïve}} = A^{-1}b$  is undesired, because it has a large component coming from the noise in the data:

$$x^{\text{na\"ive}} = A^{-1}b = A^{-1}(A\bar{x} + e) = \bar{x} + A^{-1}e.$$

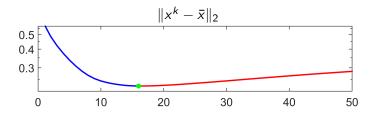
The component  $A^{-1}e$  dominates over  $\bar{x}$ , because A is ill conditioned.

#### But something interesting happens during the iterations ....

### The Reconstruction Error With Noisy Data



# Semi-Convergence



- In the initial iterations  $x^k$  approaches the unknown ground truth  $\bar{x}$ .
- During later iterations  $x^k$  converges to the undesired  $x^{\text{naïve}} = A^{-1}b$ .
- Stop the iterations when the convergence behavior changes.

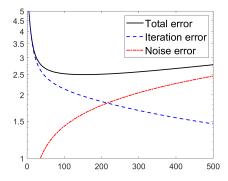
Then we achieve a regularized solution: an approximation to the noise-free solution which is not too perturbed by the noise in the data.

## Convergence Analysis: Split the Error

Let  $\bar{x}^k$  denote the iterates for a noise-free right-hand side. We consider:

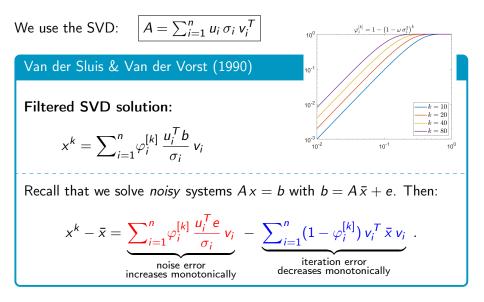


We expect the iteration error to decrease and the noise error to increase. Then we have *semi-convergence* when the noise error starts to dominate:



Convergence and Non-Convergence

# Analysis of Semi-Convergence for Landweber

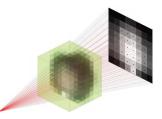


# Storage Considerations

 $N \times N$  image: each X-ray intersects at most 2N pixels  $\rightarrow$  at most 2N nonzero elements in each row of A (at most 3N in 3D)  $\rightarrow$  A is *sparse*.

Can still be problematic. 3D example: 1000 projection angles,  $1000 \times 1000$  detector pixels,  $1000 \times 1000 \times 1000$  voxels  $\rightarrow$  number of non-zeros in A is of the order  $10^{12} \sim$  several Terabytes of memory.

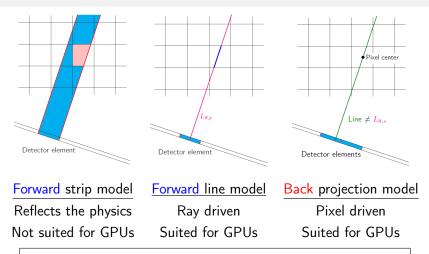
<u>Alternative</u>: use projection models to compute the matrix multiplications – the forward and back projections – "on the fly." We avoid the impossible task of storing A, at the price of having to recompute the matrix elements each time we need them.



#### More details here:



### Examples of Projection Models



Forward line model: start from detector element centers. Back projection model: start from image pixel centers and interpolate detector element values. Multiplication with  $A \iff$  action of forward projector  $\mathcal{R}$ .

Multiplication with  $B \iff$  action of back projector  $\mathcal{B} = \operatorname{adjoint}(\mathcal{R})$ .

When we can store A then we use  $A^T$  for back projection B, and our stationary iterative methods solve least squares problems associated with the normal equations  $A^T A x = A^T b$ .

When A is too large to store, we must use matrix-free multiplications of the forward projector and the back projector – cf. the Appendix.

HPC software: computational efficiency takes priority  $\rightarrow B \neq A^T$ .

We must study the influence of **unmatched** projector pairs on the computed solutions and the convergence of the iterations.

## Convergence Analysis for Unmatched Pairs

Substituting **B** for  $A^{T}$  in Landweber leads to the **BA** Iteration

$$x^{k+1} = x^k + \omega \mathbf{B} (b - \mathbf{A} x^k), \qquad \omega > 0.$$

A *fixed-point iteration* that is not related to solving a minimization problem! Any fixed point  $x^*$  satisfies the **unmatched normal equations** 

$$BAx^* = Bb.$$

#### Shi, Wei, Zhang (2011); Elfving, H (2018)

The **BA** Iteration converges to a solution of BAx = Bb if and only if

$$0 < \omega < rac{2\operatorname{\mathsf{Re}}(\lambda_j)}{|\lambda_j|^2} \quad ext{and} \quad \operatorname{\mathsf{Re}}(\lambda_j) > 0, \qquad \{\lambda_j\} = \operatorname{\mathtt{eig}}({}^{m{B}}{}^{m{A}})$$

# Iteration Error and Noise Error When $\operatorname{Re}(\lambda_j) > 0 \ \forall j$

### Elfving, H (2018)

The *iteration error* is given by

 $ar{x}^k - ar{x}^* = T^k (ar{x}^0 - ar{x}) \;, \quad ar{x}^0 = {
m initial \ vector} \;, \quad T = I - \omega \, {\it B} {\it A} \;,$ 

and it follows that we have linear convergence:

$$\|\bar{x}^k - \bar{x}\|_2 \leq \|T^k\|_2 \|\bar{x}^0 - \bar{x}\|_2 \leq \|T\|_2^k \|\bar{x}^0 - \bar{x}\|_2.$$

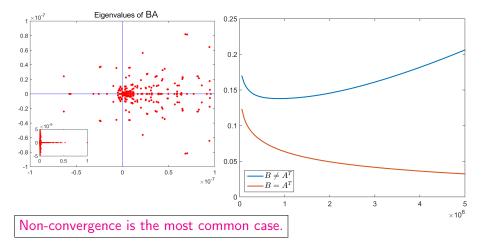
With  $b = A\bar{x} + e$  the noise error satisfies

$$\|x^k - \bar{x}^k\|_2 \le (\omega \, c \|B\|_2) \, k \, \|e\|_2$$

where we define the constant c by:  $\sup_{j} ||(I - \omega BA)^{j}||_{2} \le c$ . I.e., the upper bound grows linearly with the number of iterations k.

### Numerical Example of Non-Convergence – no Noise

Parallel-beam CT, unmatched pair from ASTRA, 64 × 64 Shepp-Logan phantom, 90 proj. angles, 60 detector pixels, min Re( $\lambda_i$ ) =  $-6.4 \cdot 10^{-8}$ .



Convergence and Non-Convergence

# What To Do?

- Ask the software developers to change their implementation of forward projection and/or back projection?
   → Significant loss of computational efficiency.
- ② Use mathematics to *fix* the nonconvergence.
   → What we do here.



We define the **shifted** version of the BA Iteration:

$$x^{k+1} = (1 - \alpha \omega) x^k + \omega \mathbf{B} (\mathbf{b} - \mathbf{A} x^k) , \qquad \omega > 0$$

with just one extra factor  $(1 - \alpha \omega)$ ; simple to implement.



Many thanks to Tommy Elfving for originally suggesting this.

# Convergence Results

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#### Dong, H, Hochstenbach, Riis (2019)

The Shifted BA Iteration converges to a fixed point if and only if  $\alpha$  and  $\omega$  satisfy

$$0 < \omega < 2 \frac{\operatorname{Re} \lambda_j + \alpha}{|\lambda_j|^2 + \alpha (\alpha + 2 \operatorname{Re} \lambda_j)} \quad \text{and} \quad \operatorname{Re} \lambda_j + \alpha > 0 .$$
  
here  $\{\lambda_j\} = \operatorname{eig}(BA).$   
he fixed point  $x_{\alpha}^*$  satisfies  
 $(BA + \alpha I) x_{\alpha}^* = Bb , \quad \bar{x} - \bar{x}_{\alpha}^* = \alpha (BA + \alpha I)^{-1} \bar{x} .$ 

This result tells us how to choose the shift parameter  $\alpha$ :

Choose  $\alpha$  just large enough that  $\operatorname{Re} \lambda_j + \alpha > 0$  for all j.

# Alternative: Solve the Unmatched Normal Equations

Instead of "fixing" a stationary method designed for solving another problem, just solve the <u>u</u>nmatched <u>n</u>ormal <u>e</u>quations in one of the forms

UNE: 
$$BAx = Bb$$
 or  $ABy = b$ ,  $x = By$ 

The left- or right-preconditioned **GMRES** method for (A, b) immediately presents itself as a good choice with *B* as the preconditioner.

<u>BA-GMRES</u> solves BAx = Bb with B as a left preconditioner.

<u>AB-GMRES</u> solves A B y = b, x = B y with B as a right preconditioner.

Advantages:

- these methods always converge,
- no need for relaxation parameter or shift parameter.

Semi-convergence: Calvetti, Lewis, Reichel (2002), Gazzola, Novati (2016).

# Solving the Unmatched Normal Equations

#### Hayami, Yin, Ito (2010)

<u>AB-GMRES</u> solves min<sub>y</sub>  $||ABy - b||_2$ , x = By (B = right precond.)

- $\min_x ||Ax b||_2 = \min_z ||ABz b||_2$  holds for all b if an only if range(B) = range(A<sup>T</sup>).
- ▶ The LS residual norm  $||Ax^k b||_2$  decreases monotonically.

<u>BA-GMRES</u> solves min<sub>x</sub>  $||BAx - Bb||_2$  (B = left preconditioner)

- ▶ the problems  $\min_x ||Ax b||_2$  and  $\min_x ||BAx Bb||_2$  are equivalent for all *b* if and only if range $(B^T)$  = range(A).
- ▶ The UNE residual norm  $||BAx^k Bb||_2$  decreases monotonically.

Both methods use the same Krylov subspace

$$span\{Bb, BABb, \ldots, (BA)^{k-1}Bb\}$$

for the solution, but they use different objective functions.

## When the Transpose Matches

#### H, Hayami, Morikuni

**AB-GMRES** with 
$$B = A^T$$
 computes  $x^k = A^T u^k$  with

$$u_k = \arg \min_{u \in \mathcal{K}_k(AA^T, b)} \|AA^T u - b\|_2^2.$$

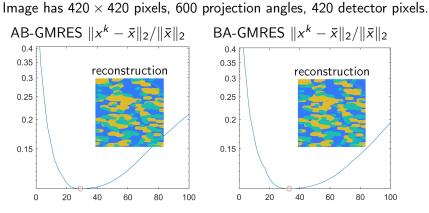
The method minimizes  $||b - Ax^k||_2$  and so do CGLS and LSQR; they produce the same iterates (in  $\infty$  precision).

**BA-GMRES** with  $B = A^T$  applies GMRES to

$$A^T A x = A^T b \qquad \longleftrightarrow \qquad \min_{x} \|A x - b\|_2 .$$

Equivalent to applying MINRES to the normal equations  $A^T A x = A^T b$  which, in turn, is equivalent to **LSMR** (in  $\infty$  precision).

# Reconstr. Error, Noisy Data, Matrix is $252\,000 \times 176\,400$



- Semi-convergence is evident.
- Same minimum reconstruction error  $||x^k \bar{x}||_2 / ||\bar{x}||_2 \approx 0.10$  for both.
- Slightly fewer iterations for AB-GMRES in this example.

# Stopping Rules

We must terminate the iterations at the point of semi-convergence.

• Discrepancy principle (DP): terminates the iterations as soon as the residual norm is smaller than the noise level:

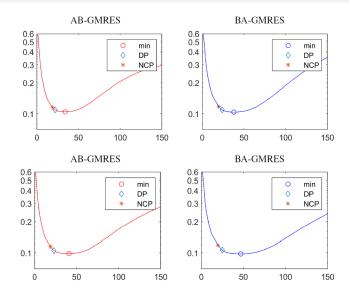
 $k_{\text{DP}}$  = the smallest k for which  $||b - Ax^k||_2 \le \tau ||e||_2$ 

where  $\tau \ge 1$  = safety factor when we have a rough estimate of  $||e||_2$ .

• NCP criterion: uses a normalized cumulative periodogram to perform a spectral analysis of the residual vector  $b - Ax^k$  and identifies when the residual is close to being white noise – indicating that all available information has been extracted from the noisy data.

For those who are curious: the L-curve criterion does not work, and we cannot implement generalized cross validation (GCV) efficiently.

# Stopping Rules: Tests With 2 Different Back Projectors



Both DP and NCP stop a bit too early – better than stopping too late.

IP Seminars, UC Irvine, 2022

Convergence and Non-Convergence

### Iterative image reconstruction for CT with unmatched projection matrices using the generalized minimal residual algorithm

Emil Y. Sidky, Per Christian Hansen, Jakob S. Jørgensen, and Xiaochuan Pan

Cone-beam CT data acquired on an Epica Pegaso veterinary CT scanner with 180 projections taken uniformly over one circular rotation, using a physical "quality assurance phantom."

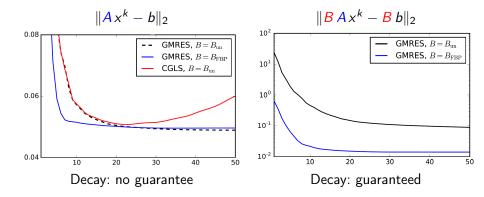
Detector: 1088  $\times$  896 pixels. Reconstruction: 1024  $\times$  1024  $\times$  300 voxels.

Ray-driven forward projector A. Two choices of back projector B:

- $B_{un} = voxel-driven$  back projection, linear interpolation on detector.
- $B_{\text{FBP}} = B_{\text{un}}F$  = filtered back-projection, where F = ramp filter.

<sup>1</sup>7th Intl Conf on Image Formation in X-Ray CT, June 12-16, 2022, Baltimore.

### Brand New Results - Convergence



BA-GMRES works well with both *B*-matrices.

"CGLS" fails to converge, because it is not CGLS.

# Coda

#### Convergence

- Good understanding of convergence for noise-free data.
- Emerging: good understanding of semi-convergence for noisy data.
- Non-convergence of stationary methods due to unmatched projectors.
- Can be fixed  $\rightarrow$  shifted BA iteration.
- Not an issue for AB-GMRES and BA-GMRES.

Method	+	_
Shifted BA	no extra storage	2 parameters $\omega$ and $\alpha$
ABBA GMRES	no extra parameters	storage for Arnoldi vectors

#### Future

- More theory about semi-convergence for GMRES.
- Deal with GMRES memory issue: restart, recycling, etc.
- Ready-to-use implementations for the CT community.